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(19) **United States**(12) **Patent Application Publication****Abdul-Hafiz et al.**(10) **Pub. No.: US 2004/0039272 A1**(43) **Pub. Date: Feb. 26, 2004**(54) **LOW NOISE OPTICAL HOUSING****Publication Classification**(76) Inventors: **Yassir Abdul-Hafiz**, Irvine, CA (US);
John Schmidt, Lake Forest, CA (US)(51) **Int. Cl.⁷ A61B 5/00**(52) **U.S. Cl. 600/322**

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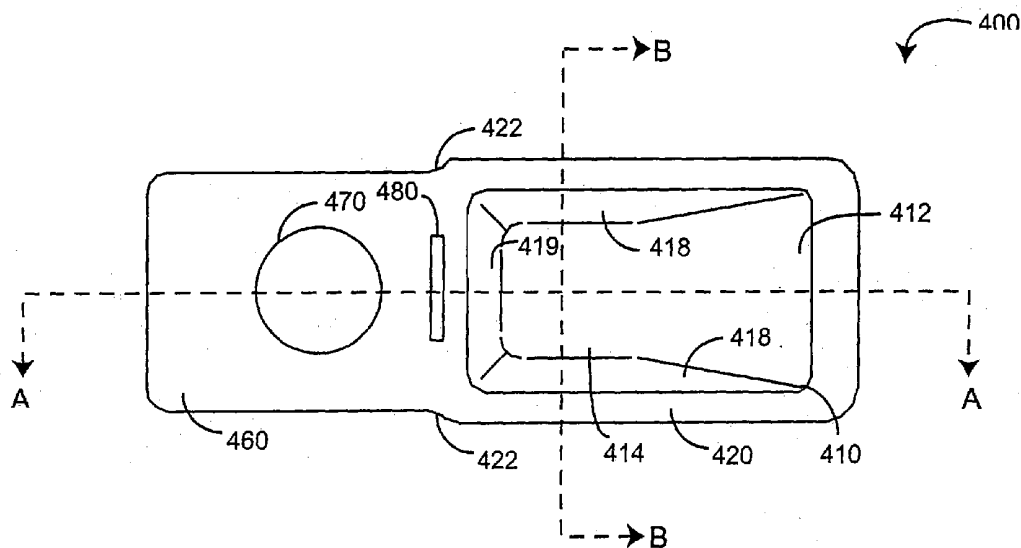
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ABSTRACT

Aspects of the invention include an optical housing including a substrate having a reflective side and an absorbing side. The substrate has a generally planar base portion and a protruding cover portion. The cover portion defines a pocket on the absorbing side. The substrate has an open position where the base portion is distal the cover and a closed position where the base portion is proximate the cover. The substrate is configured to enclosed a detector within the pocket in the closed position. The base portion defines an aperture generally centered within the base portion and aligned with the detector in the closed position so as to pass light through to the detector.

(21) Appl. No.: **10/632,012**(22) Filed: **Jul. 31, 2003****Related U.S. Application Data**

(60) Provisional application No. 60/400,177, filed on Aug. 1, 2002.



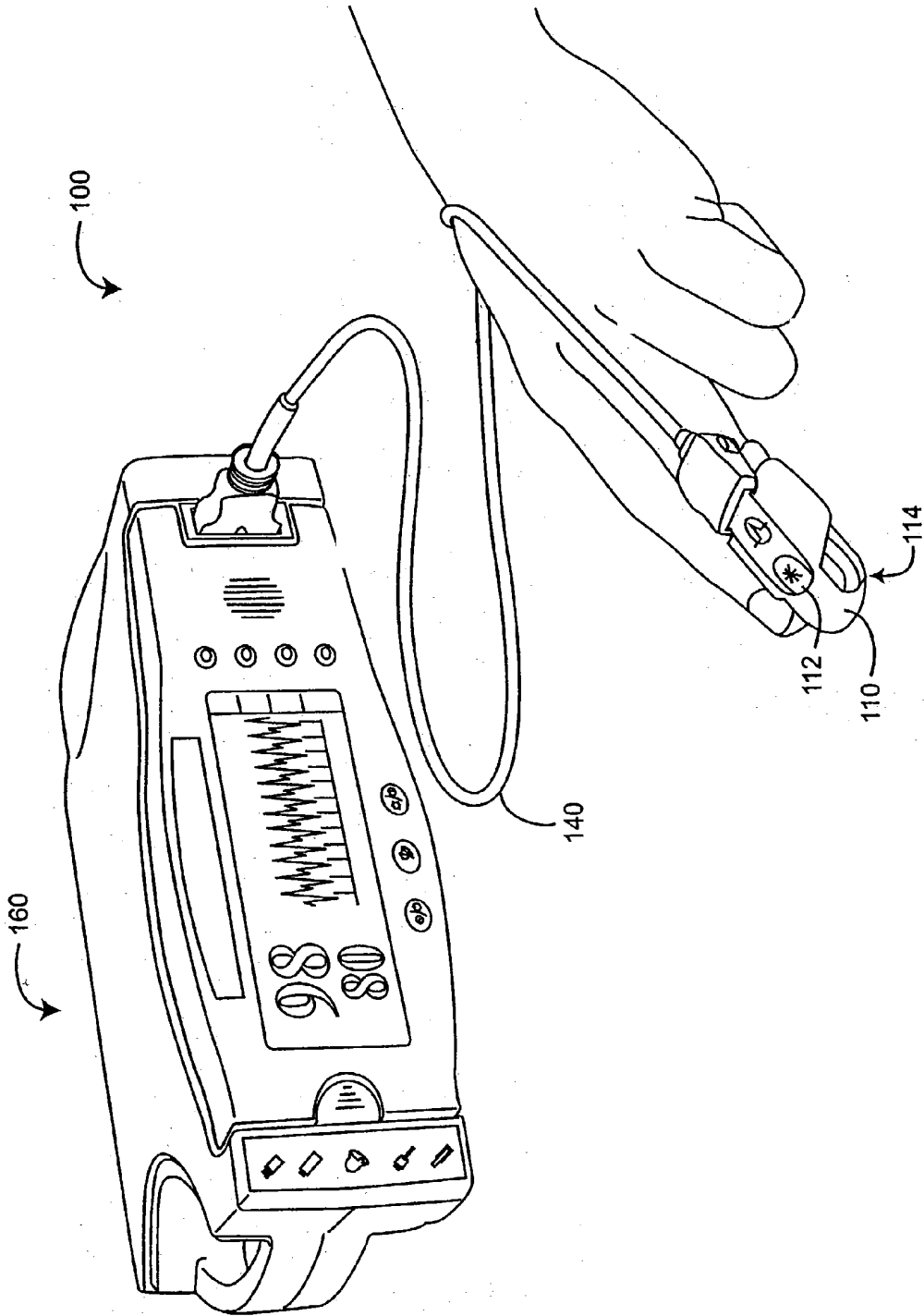


FIG. 1 (Prior Art)

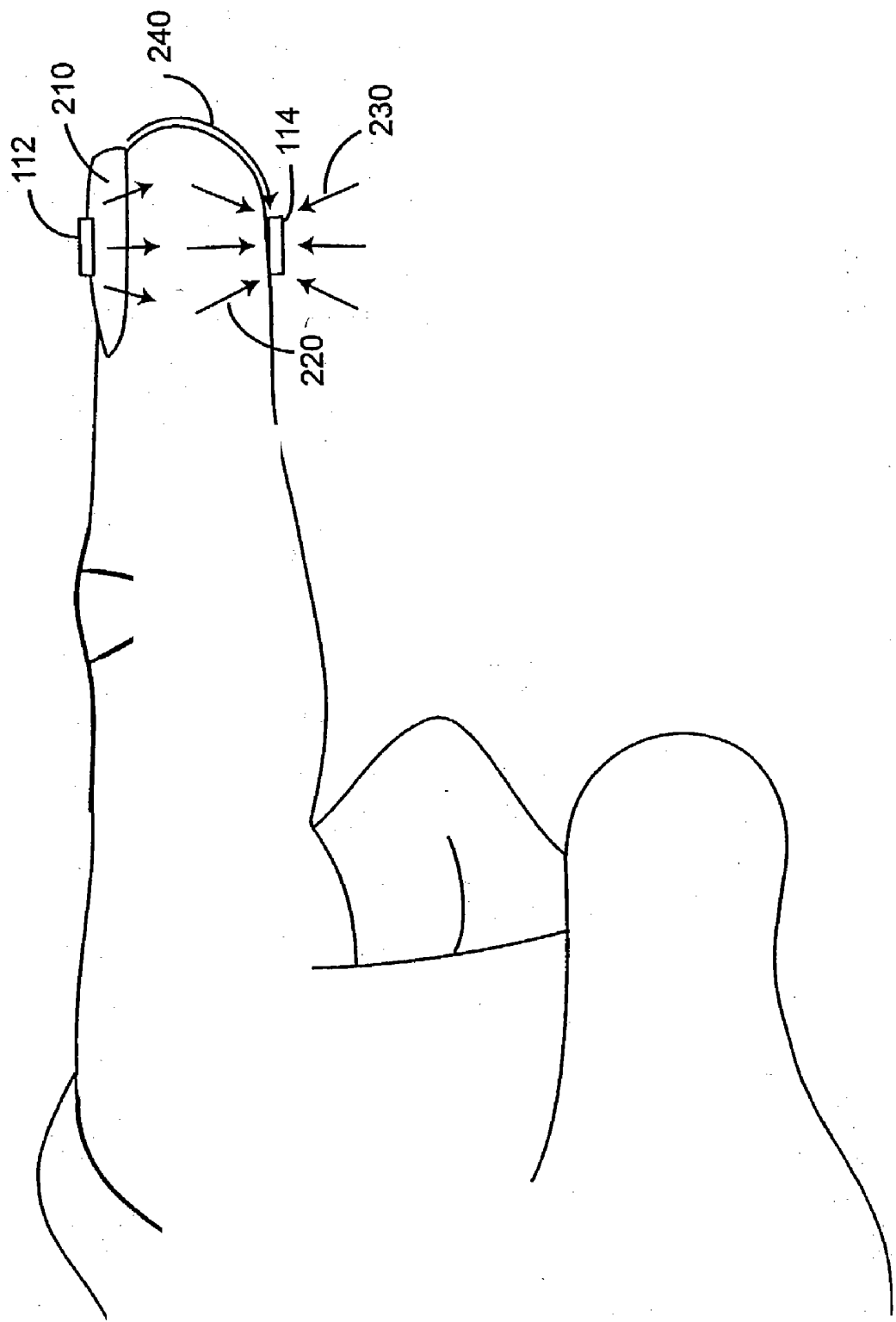


FIG. 2 (Prior Art)

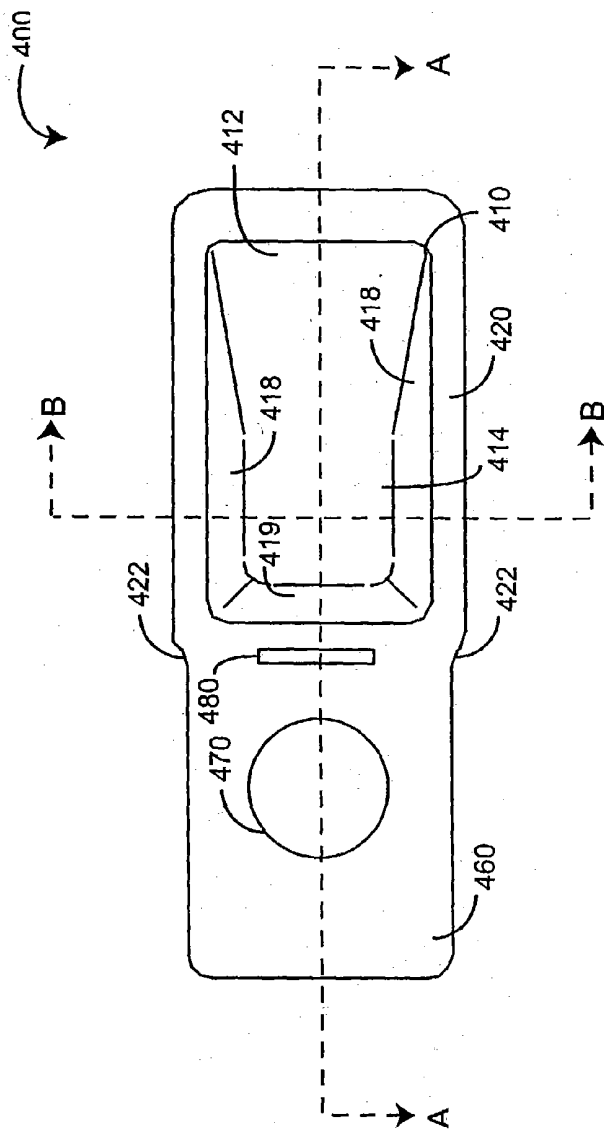


FIG. 4A

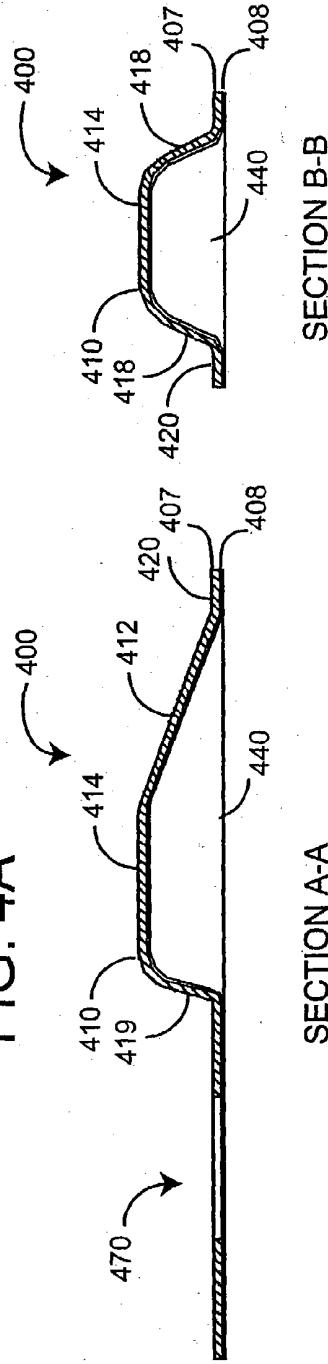


FIG. 4B

FIG. 4C

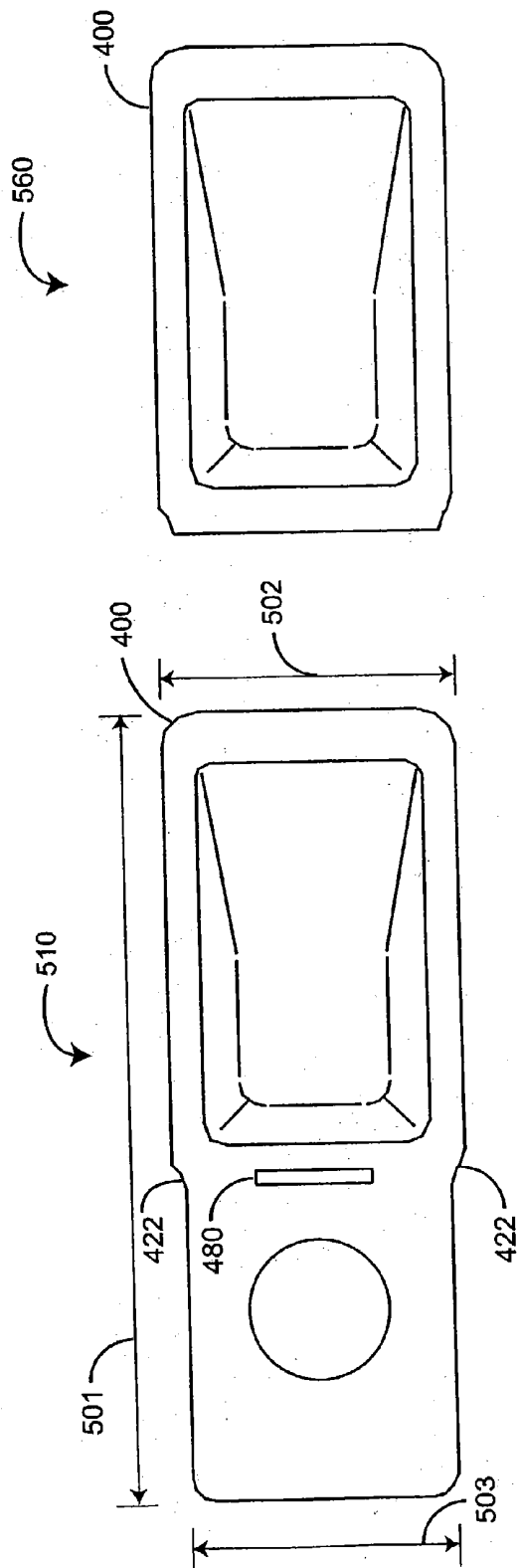


FIG. 5C

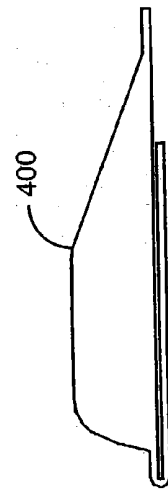


FIG. 5D

FIG. 5A

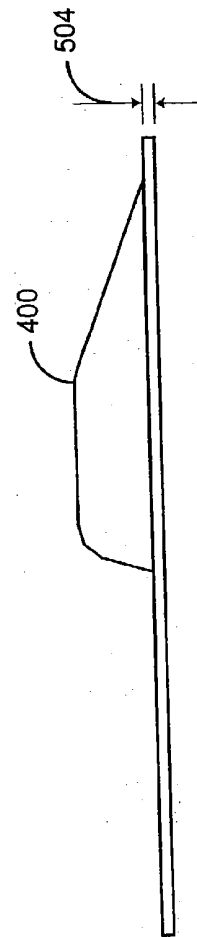


FIG. 5B

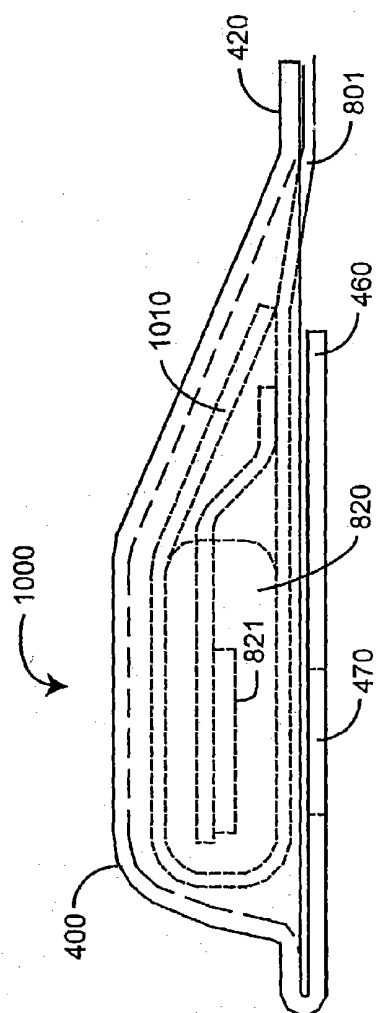


FIG. 6A

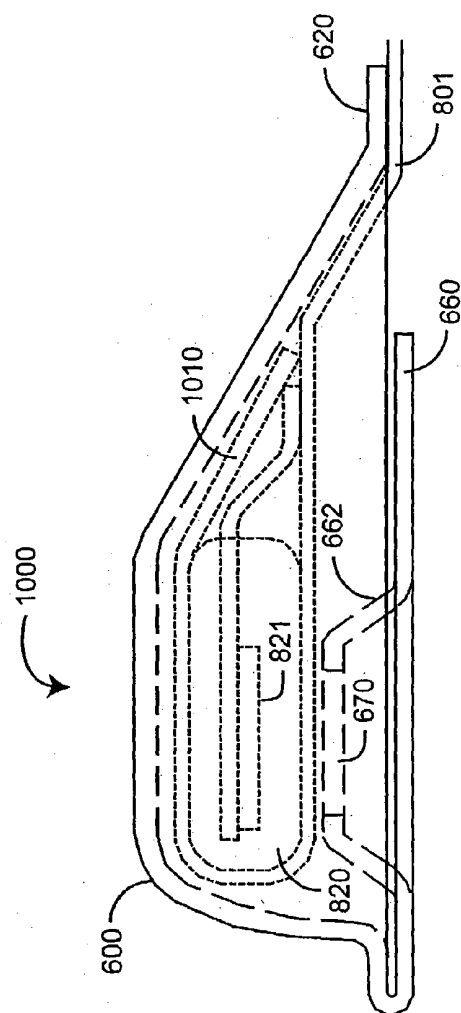


FIG. 6B

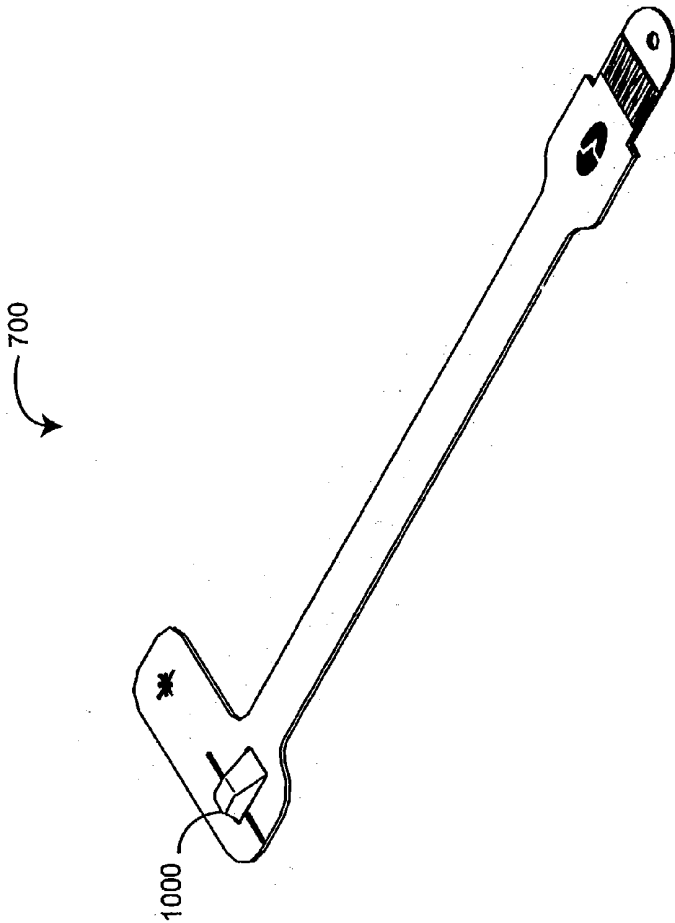


FIG. 7B

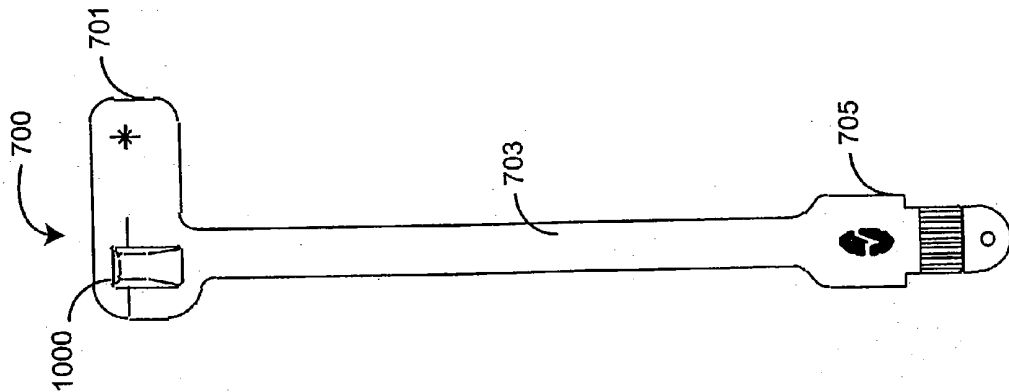


FIG. 7A

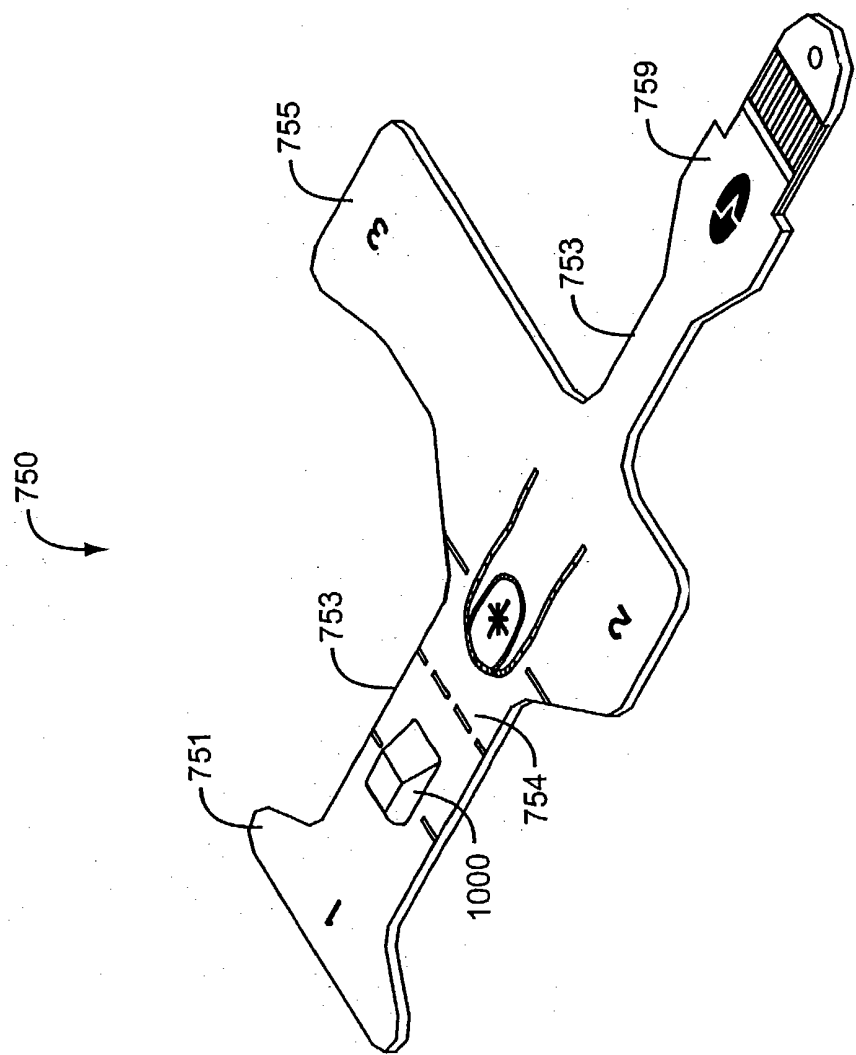


FIG. 7C

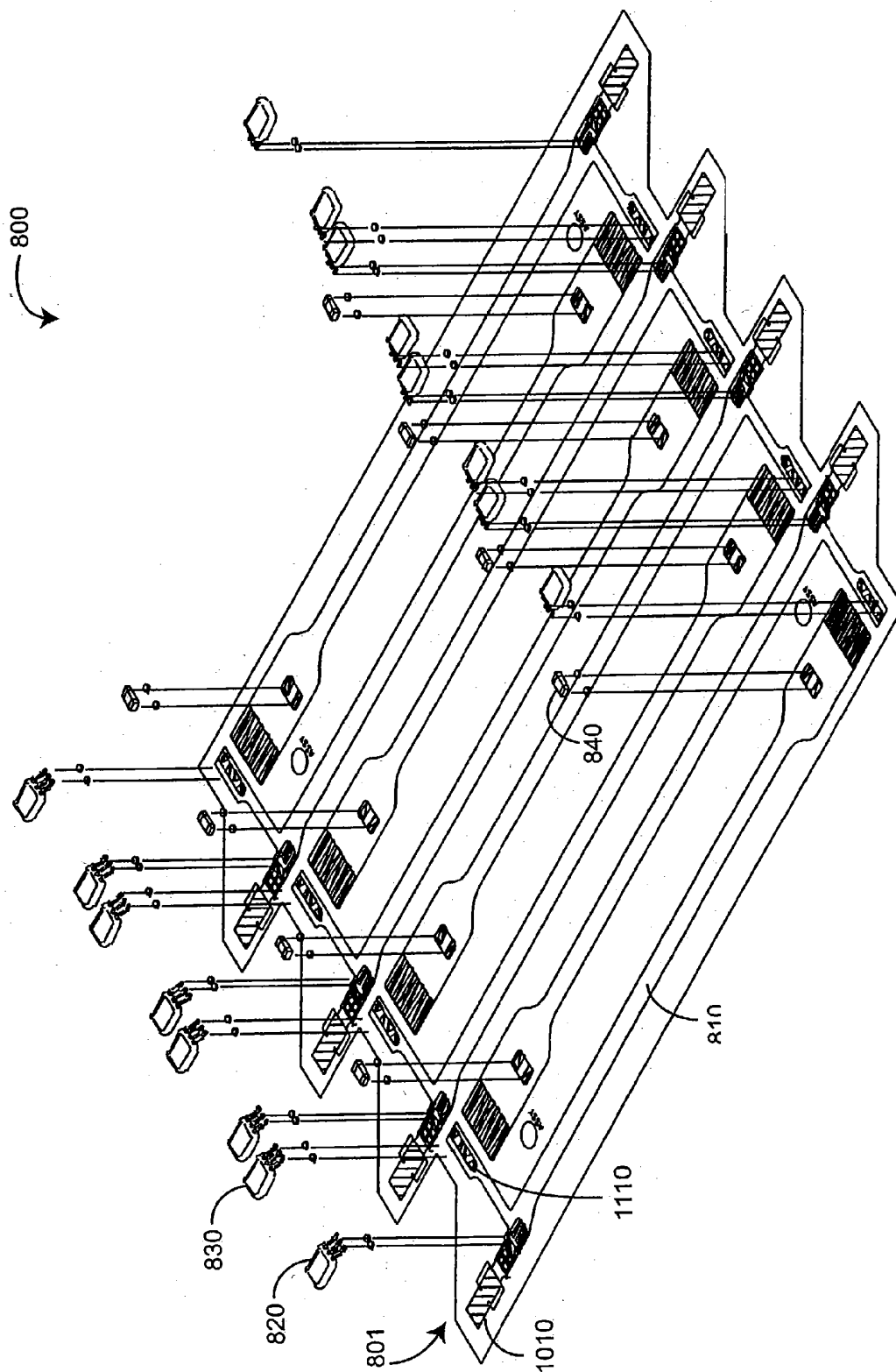


FIG. 8A

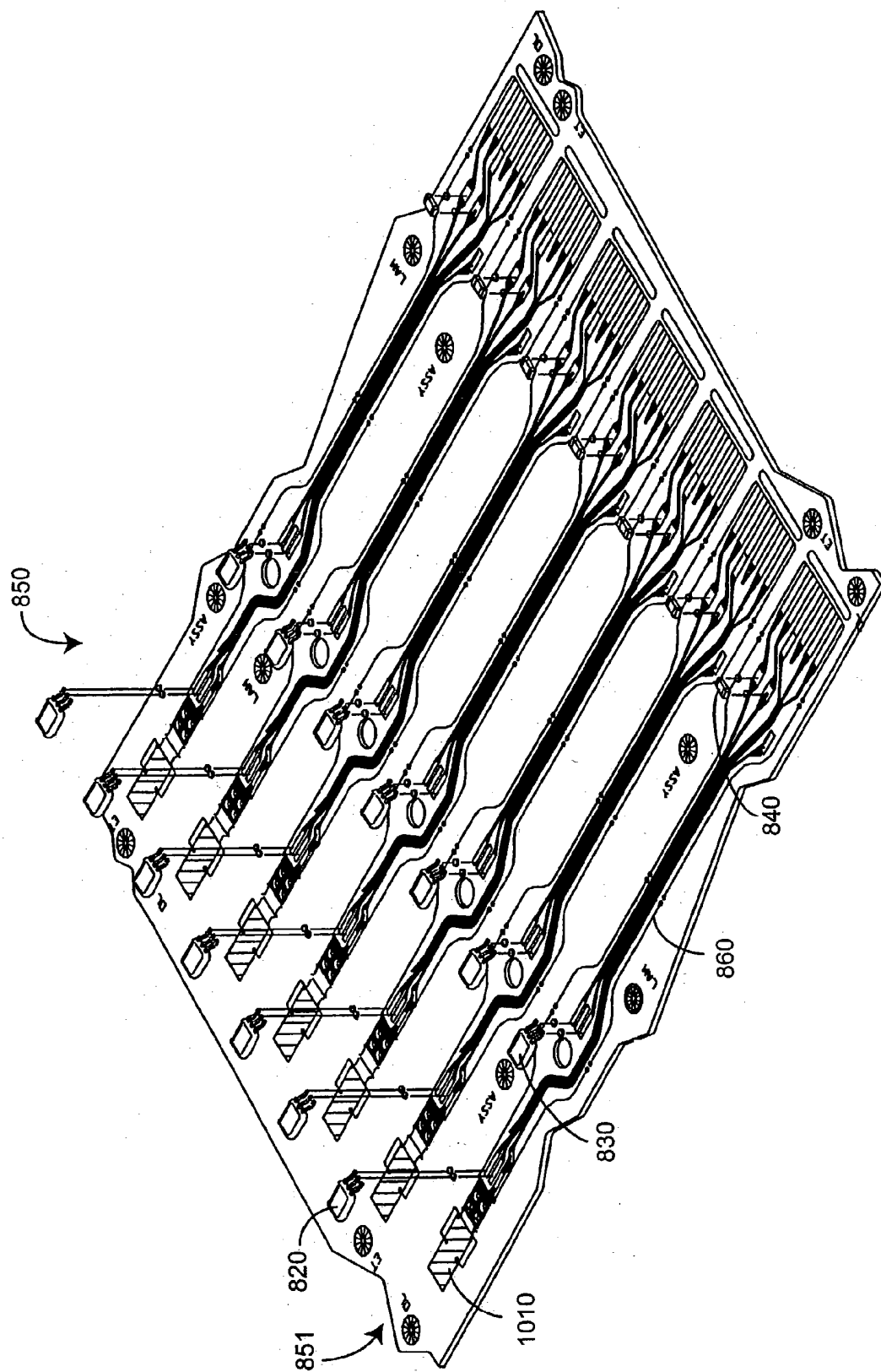
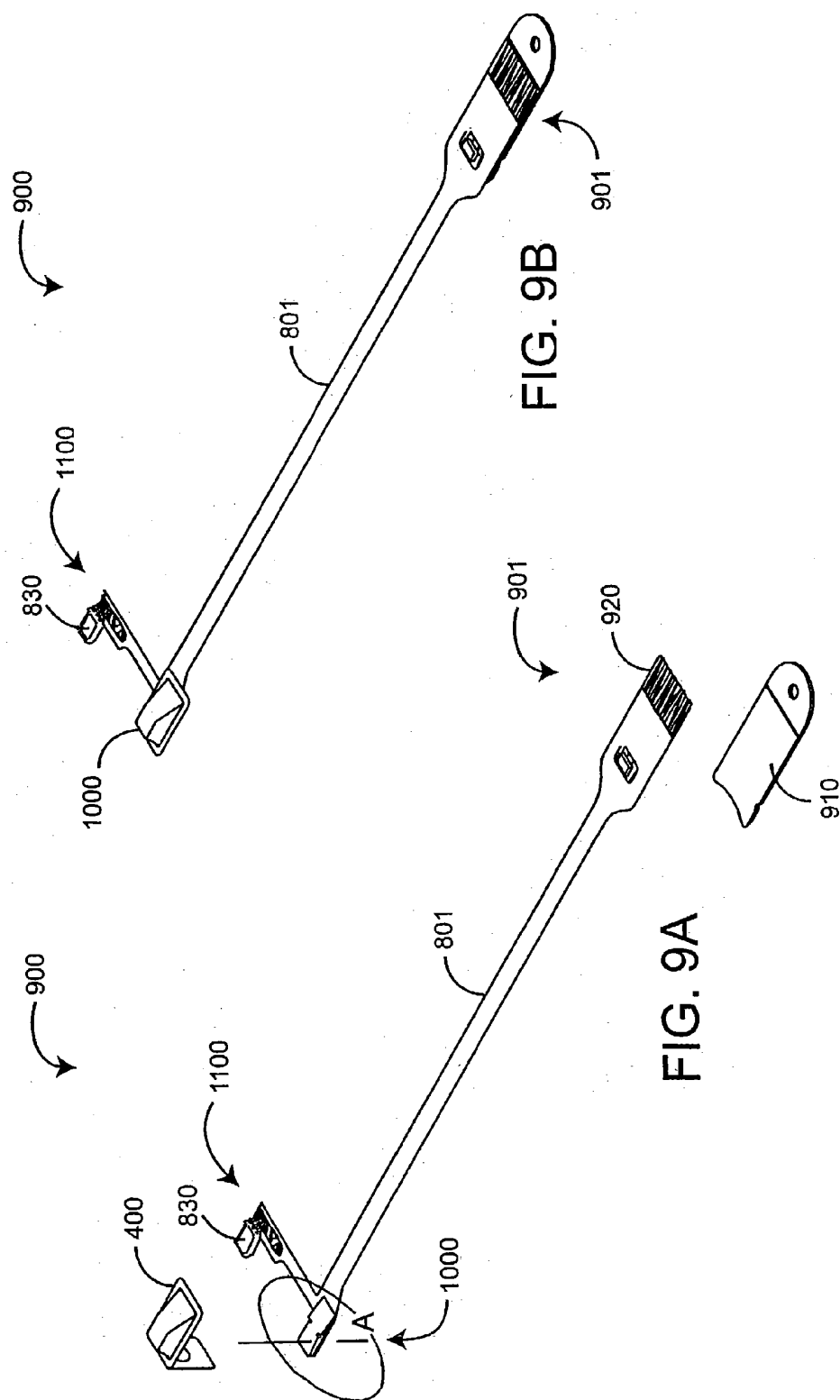
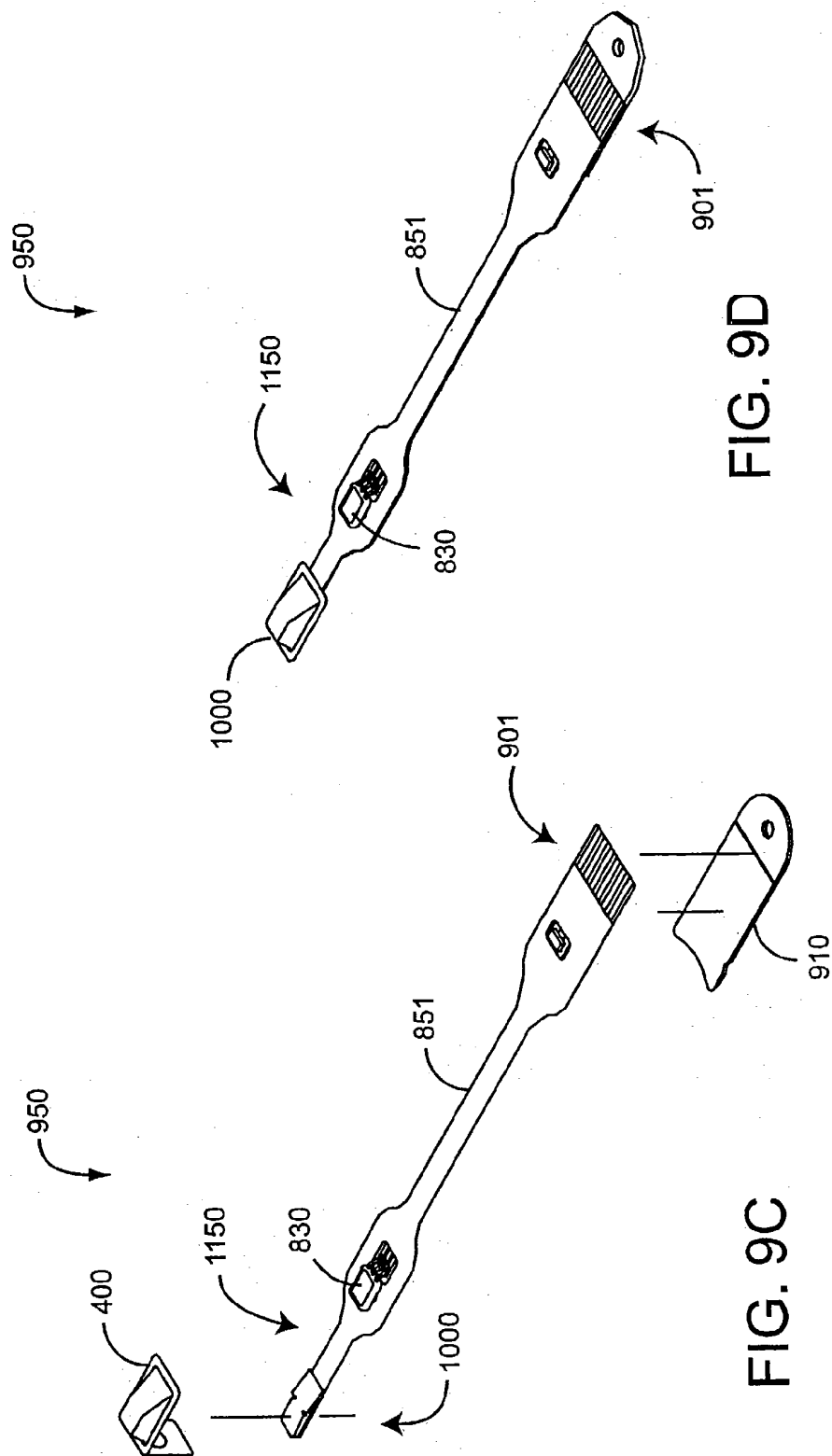
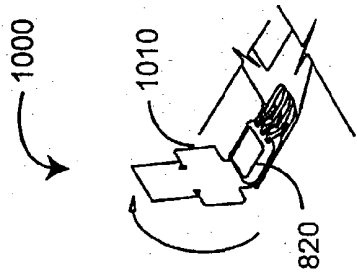


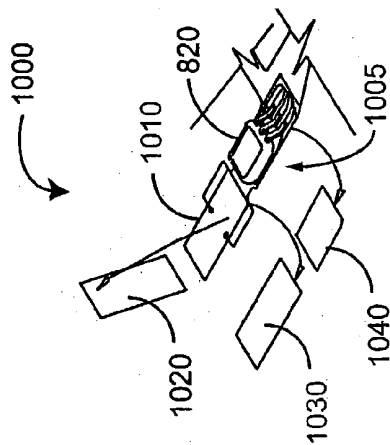
FIG. 8B



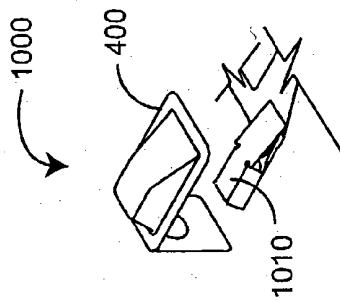




DETAIL A
FIG. 10B



DETAIL A
FIG. 10A



DETAIL A
FIG. 10C

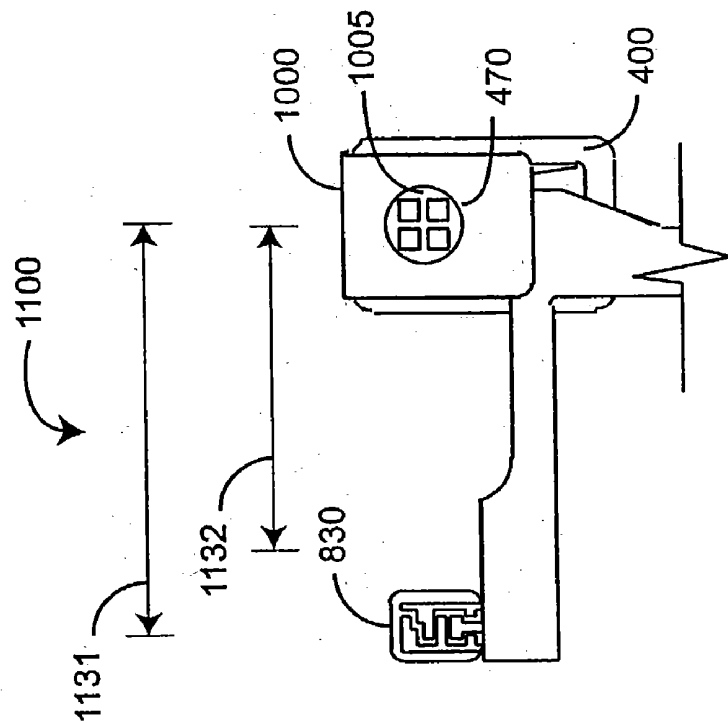


FIG. 11B

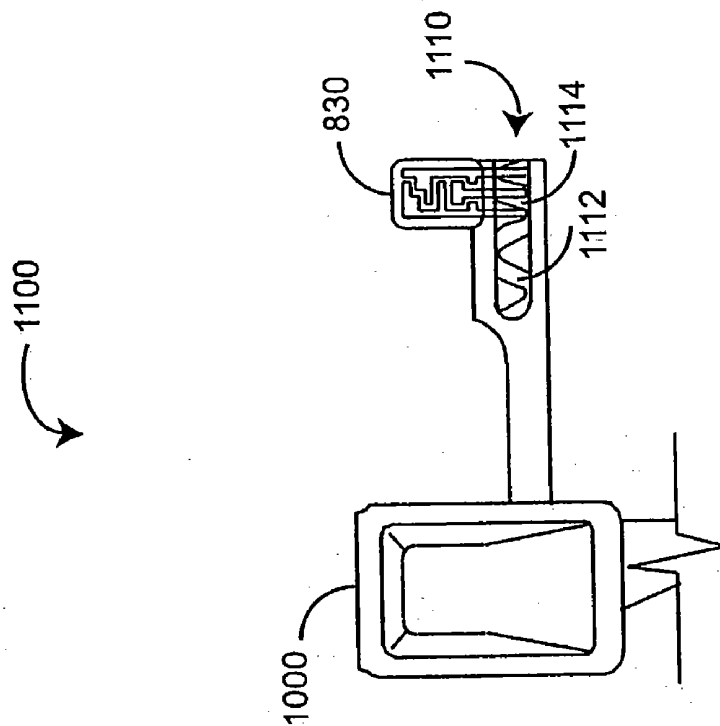


FIG. 11A

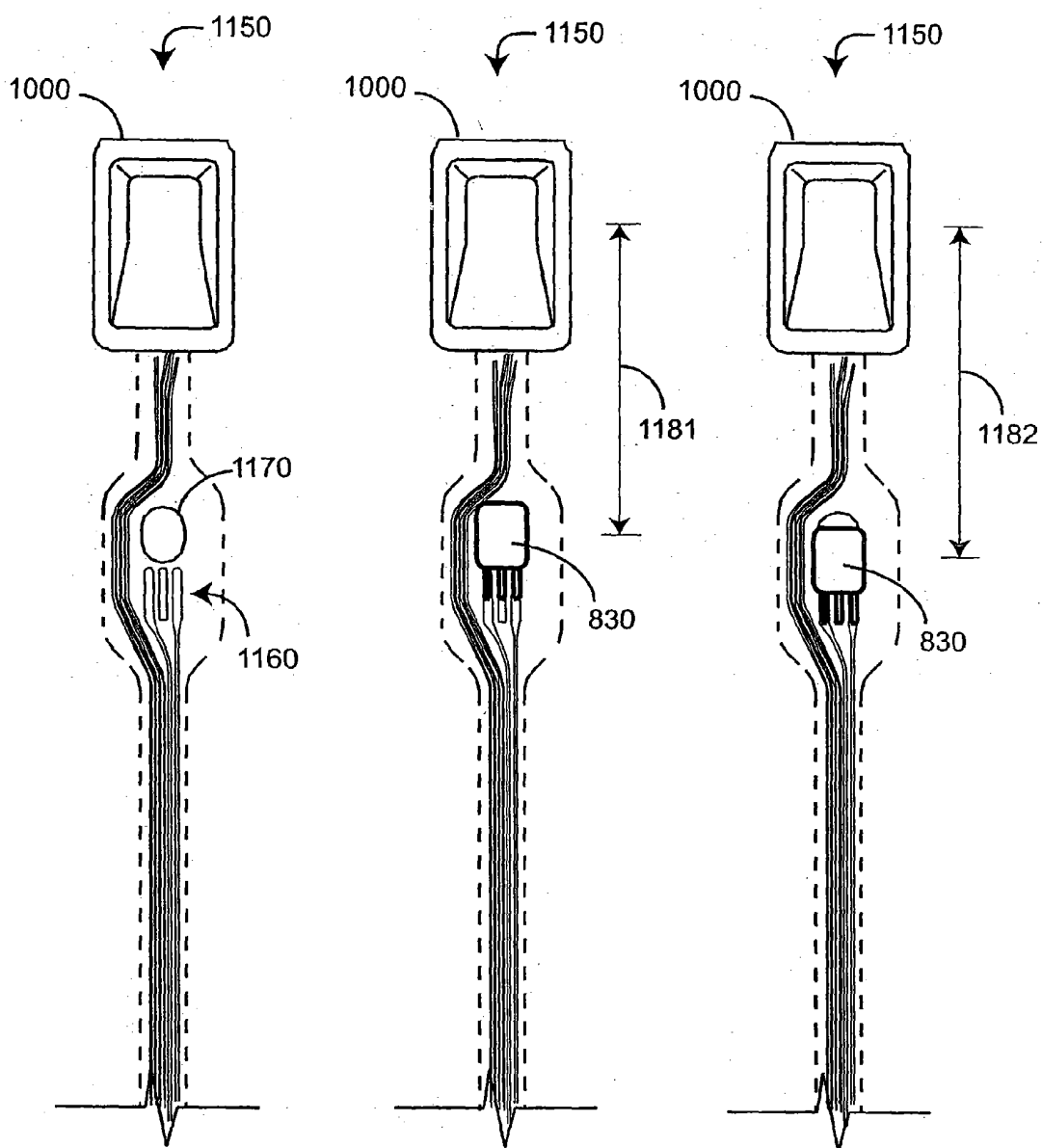


FIG. 11C

FIG. 11D

FIG. 11E

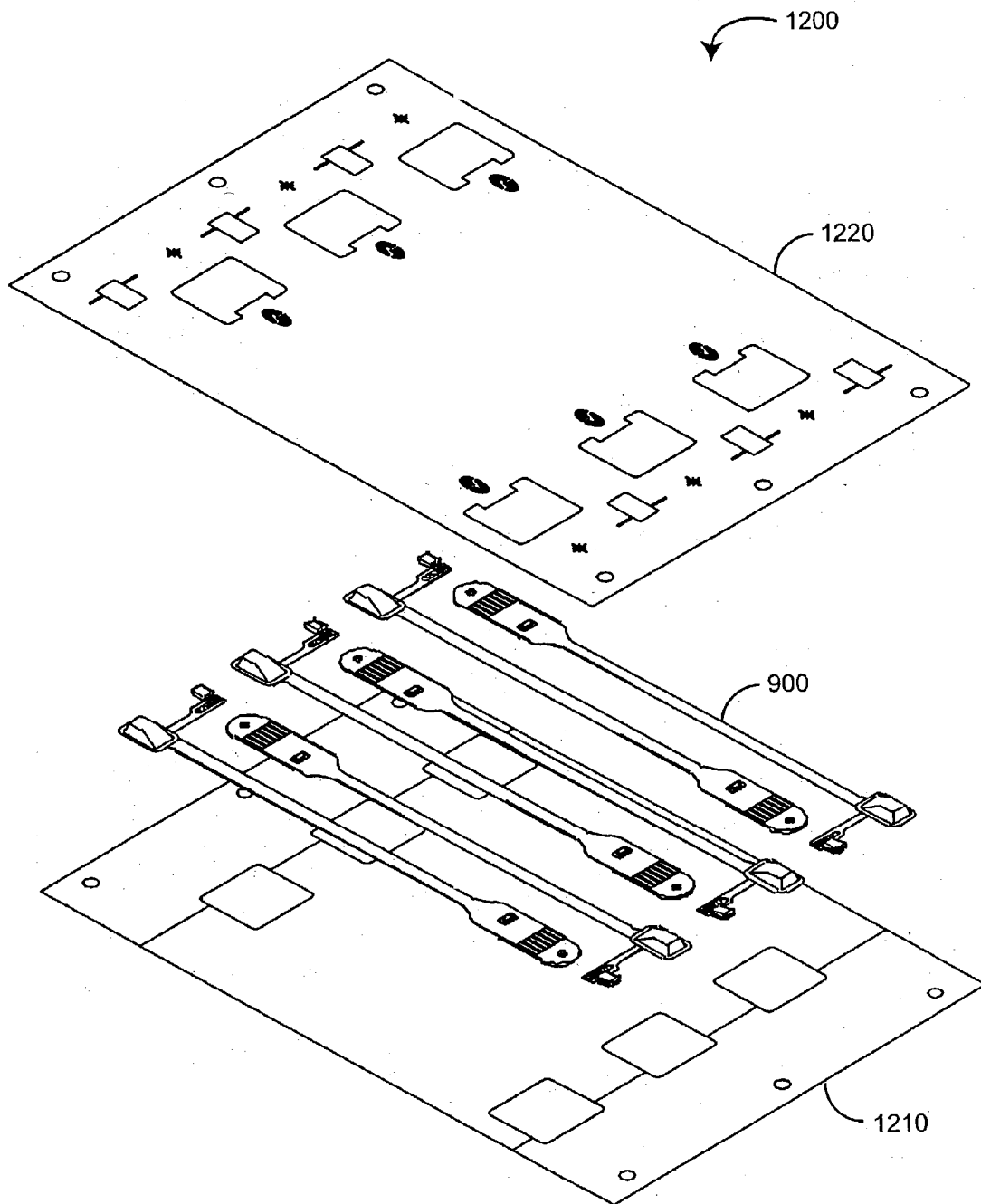


FIG 12A

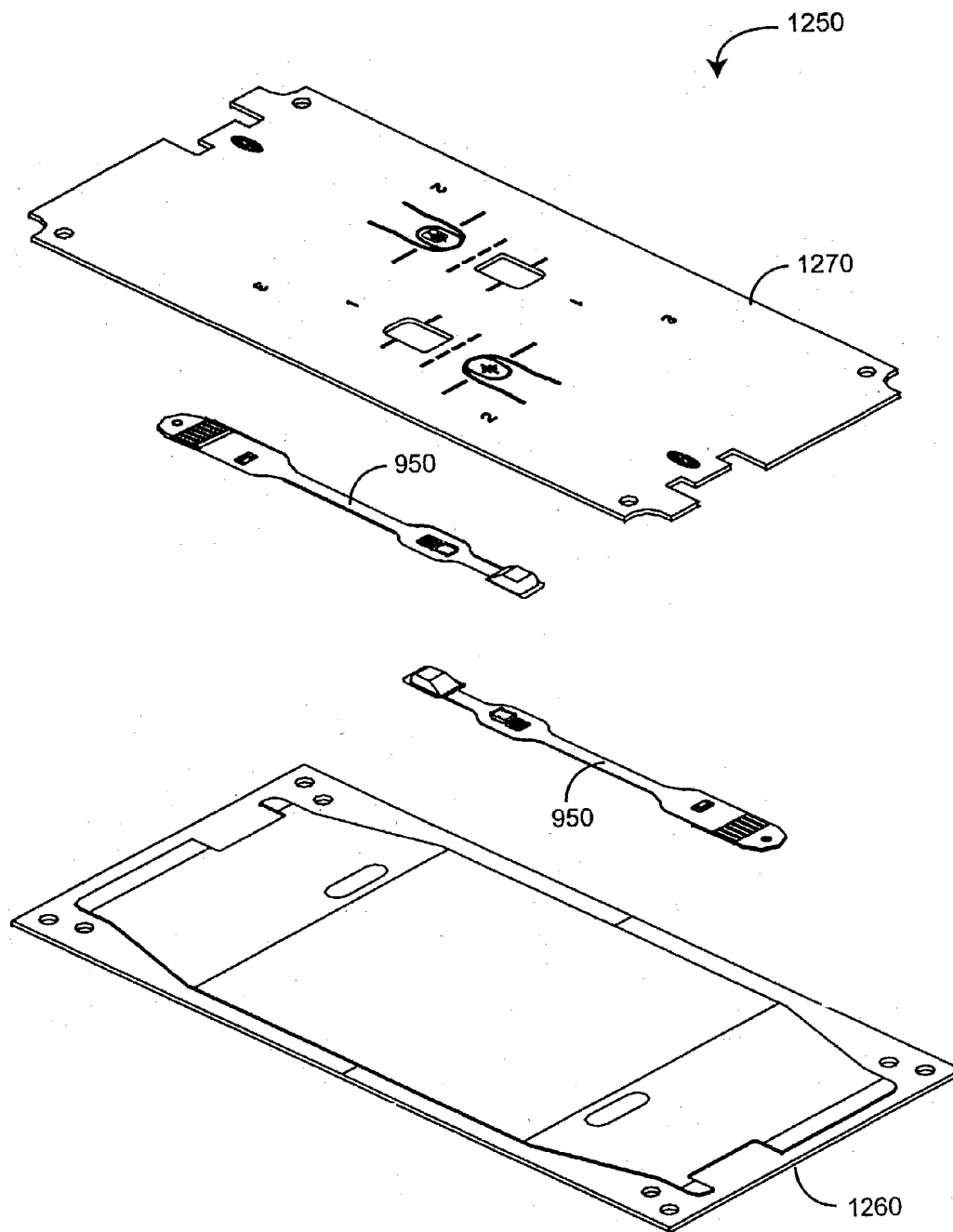


FIG. 12B

LOW NOISE OPTICAL HOUSING

REFERENCE TO RELATED APPLICATION

[0001] This application claims the benefit of U.S. Provisional Application No. 60/400,177, Aug. 1, 2002. The present application incorporates the foregoing disclosures herein by reference.

BACKGROUND OF THE INVENTION

[0002] Pulse oximetry is a widely accepted noninvasive procedure for measuring the oxygen saturation level of arterial blood, an indicator of a person's oxygen supply. Early detection of low blood oxygen level is critical in the medical field, for example in critical care and surgical applications, because an insufficient supply of oxygen can result in brain damage and death in a matter of minutes. FIG. 1 illustrates a pulse oximetry system 100 having a sensor 110 applied to a patient, a monitor 160 and a patient cable 140 connecting the sensor 110 and the monitor 160. The sensor 110 is attached to a tissue site, such as an adult patient's finger (as shown). Other sensor types are configured to attach, say, to a neonatal patient's foot. The sensor 110 is configured with both red and infrared LEDs 112 (hidden) that, for finger attachment, project light through the fingernail and into the blood vessels and capillaries underneath. A photodiode 114 (not visible) is positioned at the finger tip opposite the fingernail so as to detect the LED emitted light as it emerges from the finger tissues.

SUMMARY OF THE INVENTION

[0003] FIG. 2 illustrates various optical noise sources for a sensor 110 (FIG. 1). Shown is the placement of the sensor LEDs 112 and detector 114 on a finger without showing the associated electrical interconnections, base stock and face stock materials. Emitted light 210 is projected from the LEDs 112 into the fingernail bed. Received light 220 propagates through the finger tissues to the detector 114, subject to absorption and scattering, to generate a desired sensor signal. Light which illuminates the detector 114 without propagating through the finger is unwanted optical "noise" that corrupts the desired sensor signal. Noise sources include ambient light 230 and piped light 240. Ambient light 230 is transmitted to the detector 114 from external light sources, i.e. light sources other than the LEDs 112. Piped light 240 is stray light from the LEDs 112 that is transmitted around a tissue site along a light conductive surface, such as a reflective inner surface of face stock material, directly to the detector 114. Light piping and light piping reduction are described in U.S. Pat. No. 5,782,757 entitled "Low Noise Optical Probe," which is assigned Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

[0004] FIG. 3 illustrates a prior art low noise sensor 300. The sensor 300 has a detector 310, a spacer 330 and an optical shield 350. The detector 310 is configured to receive light 220 that has propagated through a tissue site 10, as described with respect to FIGS. 1-2, above. The spacer 330 is positioned between the tissue site 10 and the detector 310, providing an optical barrier so as to reduce the intensity of piped light 240 that reaches the detector 310. The spacer 330 defines an aperture 332 that allows a transmitted portion 360 of propagated light 220 to reach the detector 310. A blocked portion 370 of propagated light 220 is reflected back into the

tissue and/or absorbed by the spacer 330, depending upon the spacer material. The optical shield 350 may be a metal foil or other opaque material that prevents ambient light 230 from reaching the detector 310. Further, the detector 310, spacer 330 and optical shield 350 may be enclosed in a housing (not shown) of opaque material that further prevents ambient light 230 from reaching the detector 310. A low noise sensor is described in U.S. Pat. No. 5,782,757, cited above.

[0005] One aspect of a low noise optical housing is a substrate having a reflective side and an absorptive side. The substrate has a generally planar base portion and a protruding cover portion. The cover portion defines a pocket on the absorptive side. The substrate has an open position with the base portion distal the cover portion and a closed position with the base portion proximate the cover portion. The substrate is configured to enclosed a detector within the pocket in the closed position. The base portion defines an aperture generally centered within the base portion and aligned with the detector in the closed position so as to pass light through to the detector.

[0006] Another aspect of a low noise optical housing is a method comprising the steps of providing a substrate having an absorptive side and a reflective side and forming a cover portion of the substrate so as to create a pocket on the absorptive side. Further steps include punching the substrate so as to separate a housing from the substrate, securing a the pocket, and enclosing the detector with the housing.

[0007] A further aspect of a low noise optical housing comprises a light reflecting cover means for shielding against ambient light and a base means for blocking piped light. The base means adjoins the cover means. The housing also comprises a light absorbing pocket means for securing a detector. The pocket means is defined by the cover means and the base means. The housing further comprises an aperture means for allowing light transmitted through a tissue site to be received by the detector. The aperture means is defined by the base means.

[0008] One aspect of a sensor circuit comprises a circuit substrate, a pair of pads disposed on an optical portion of the circuit substrate, a plurality of pinouts disposed on a connector portion of the circuit substrate, and a plurality of conductive paths providing electrical communication between the pads and the pinouts. The pads are configured to mechanically mount a corresponding pair of optical components to the circuit substrate and to electrically connect the components to the conductive paths. At least one of the pads is adapted to mount one of the components at either a first spacing or a second spacing from another one of the components. The second spacing is greater than the first spacing by a predetermined mount.

[0009] Another aspect of a sensor circuit comprises a flexible circuit substrate, a first pad disposed on the circuit substrate and configured to mount a detector, and a second pad disposed on the circuit substrate and configured to mount an emitter. At least one of the first pad and the second pad are adapted so that a detector-emitter spacing is a first distance or a second distance depending on the placement of at least one of the detector and the emitter. The first distance and the second distance are predetermined so as to accommodate particular sensor types.

[0010] A further aspect of a sensor circuit is a method comprising the step of predetermining a plurality of optical

component spacings based upon a corresponding plurality of sensor types. The sensor types are indicative of tissue site location and patient size. Further steps are configuring a pad to fixedly mount and electrically connect an optical component to a flexible circuit at a plurality of positions, where the positions correspond to the spacings, and mounting the optical component to a particular one of the positions to construct a particular one of the sensor types.

[0011] An additional aspect of a sensor circuit is a sensor comprising a circuit substrate means for mounting and electrically connecting components and a pad means disposed on the circuit substrate for fixedly mounting an emitter at either a first spacing or at a second spacing from a detector. The sensor also comprises a tape stock means for attaching the emitter and the detector to a tissue site.

[0012] For purposes of summarizing the invention, certain aspects, advantages and novel features of the invention have been described herein. Of course, it is to be understood that not necessarily all such aspects, advantages or features will be embodied in any particular embodiment of the invention.

BRIEF DESCRIPTION OF THE DRAWINGS

[0013] A general architecture that implements the various features of the invention will now be described with reference to the drawings. The drawings and the associated descriptions are provided to illustrate embodiments of the invention and not to limit the scope of the invention. Throughout the drawings, reference numbers are re-used to indicate correspondence between referenced elements. In addition, the first digit of each reference number indicates the figure in which the element first appears.

[0014] FIG. 1 is a perspective view of a prior art pulse oximetry system;

[0015] FIG. 2 is a diagram illustrating optical noise sources and a prior art sensor;

[0016] FIG. 3 is a diagram illustrating optical noise sources and a prior art reduced noise sensor;

[0017] FIGS. 4A-C are top, side cross-section and front cross-section views, respectively, of a low noise optical housing;

[0018] FIGS. 5A-B are top and side views of a low noise optical housing in an open position;

[0019] FIGS. 5C-D are top and side views of a low noise optical housing in a closed position;

[0020] FIGS. 6A-B are detailed side views of alternative embodiments of a low noise optical housing enclosing a detector;

[0021] FIGS. 7A-B are top and perspective views, respectively, of an assembled pulse oximetry sensor configured for a neonate and incorporating a low noise optical housing;

[0022] FIG. 7C is a perspective view of an assembled pulse oximetry sensor configured for an adult and incorporating a low noise optical housing;

[0023] FIGS. 8A-B are exploded perspective views of neonate and adult flexible circuit assemblies, respectively, configured for a low noise optical housing;

[0024] FIGS. 9A-B are perspective views of a neonate sensor assembly showing installation of a low noise optical housing;

[0025] FIGS. 9C-D are perspective views of an adult sensor assembly showing installation of a low noise optical housing;

[0026] FIGS. 10A-C are detailed perspective views of an unassembled, a partially assembled and a fully assembled EMI shield, respectively, prior to low noise optical housing installation;

[0027] FIGS. 11A-B are detailed top and bottom views of a neonate or infant sensor optical assembly;

[0028] FIGS. 11C-E are detailed top views of an adult or pediatric sensor optical assembly;

[0029] FIG. 11C shows an optical assembly without the emitter installed;

[0030] FIG. 11D shows an optical assembly with pediatric detector-emitter spacing; and

[0031] FIG. 11E shows an optical assembly with adult detector-emitter spacing; and

[0032] FIGS. 12A-B are exploded perspective views of multiple neonate sensor and adult sensor assemblies, respectively, showing base stock and face stock installation.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

[0033] FIGS. 4A-C illustrate a low noise optical housing 400 having a protruding cover 410, a generally flat flange 420 disposed around the periphery of the cover 410, and a generally flat base 460 adjoining the flange 420. The housing 400 is configured to accept a detector 820 (FIGS. 6A-B) and provide ambient light and piped light reduction. In particular, the low noise optical housing 400 advantageously incorporates the functions of a light barrier, opaque cover, spacer and aperture, as described with respect to FIG. 3, above, in a relatively small, easy to manufacture, one-piece design.

[0034] As shown in FIGS. 4B-C, the housing 400 is advantageously constructed of a flat substrate which, in one embodiment, is a laminate of two materials including an outer white layer 407 and an inner black layer 408. By utilizing a laminate of both white and black material, the low noise optical housing 400 advantageously functions both as a light absorber and as a light reflector. The white layer 407 acts as a reflector, reflecting unwanted ambient light outward from a detector enclosed in the housing, as described below, as well as reflecting emitter source light back into a patient tissue site. The reflected ambient light reduces noise and the reflected source light increases the sensor current transfer ratio. The black layer 408 absorbs unwanted ambient light, preventing it from reaching the enclosed detector 820 (FIGS. 6A-B). The two materials 407, 408 are laminated together before the housing 400 is formed and shaped. The housing 400 is vacuum formed on a flat blank of the laminated material to create a cover 410, as described below. The housing 400, aperture 470 and slot 480, as described below, are then punched out and the housing 400 is removed from the remainder of the laminated material.

[0035] In an alternative embodiment, the housing 400 is formed from a black substrate, which is painted white on the

outside, i.e. the side corresponding to the outer white layer 407, or otherwise coated on the outside with a reflecting material or substance. In another alternative embodiment, the housing 400 is formed from a white substrate, which is painted black on the inside, i.e. the side corresponding to the inner black layer 408, or otherwise coated on the inside with an absorbing material or substance.

[0036] As shown in FIGS. 4A-C, the cover 410 has a ramp 412 sloping from the flange 420 to a generally level platform 414 raised above the flange 420. The cover 410 also has beveled sides 418 and a beveled back 419 that slope from the flange 420 inward to the platform 414. The cover 410 defines an pocket 440 for securing a detector 820 (FIGS. 6A-B), as described below. The flange 420 has indents 422 that gradually taper from the wider flange width 502 (FIG. 5A) to that of the narrower base width 503 (FIG. 5A).

[0037] Also shown in FIGS. 4A-C, the base 460 defines a generally centered aperture 470 and a slot 480 proximate the flange 420, partially extending across the base width 503 (FIG. 5A). In a closed position, as described with respect to FIGS. 5C-D, below, the base 460 provides a bottom for the cover 410 and pocket 440 and optically shields the detector 820 (FIGS. 6A-B). The base 460 also provides a spacer and aperture to reduce light piping. The slot 480 allows the base 460 to be easily folded so that the aperture 470 is in proper alignment with the detector active area. Further, the narrower base width 503 (FIG. 5A) allows the flange 420 to overlap the base 460 in the closed position 560 (FIGS. 5C-D) so as to seal the housing edges from ambient light. The flange 420 also provides structure for attaching the housing 400 to a tape stock layer (FIGS. 12A-B).

[0038] FIGS. 5A-D illustrate the housing 400 in an open position 510 (FIGS. 5A-B) and a closed position 560 (FIGS. 5C-D). As shown in FIGS. 5A-B, in an open position 510 the housing 400 has an overall length 501, a flange width 502, a base width 503 and a thickness 504. The flange width 502 is greater than the base width 503. In one embodiment, the housing length 501 is less than about 1.1 inches, the flange width 502 is less than about 0.4 inches and the housing thickness 504 is less than about 0.015 inches. As shown in FIGS. 5A-D, from an open position 510, the housing 400 is folded to the closed position 560 along the slot 480 and across the base width 503 proximate to each indent 422. In the closed position 560, the housing 400 provides an optical enclosure for a detector, as described with respect to FIGS. 6A-B, below.

[0039] FIGS. 6A-B illustrate shielded detector assemblies 1000 incorporating flat aperture 400 and raised aperture 600 embodiments, respectively, of a low noise optical housing. A detector 820 is enclosed in the optical housing 400, 600 so that the active area of the photodiode chip 821 is aligned with the housing aperture 470, 670. An EMI shield 1010, described with respect to FIGS. 10A-C, below, also encloses the detector 820, and a corresponding flexible circuit assembly 801, described with respect to FIGS. 8-9, below, exits the housing 400, 600 between the base 460, 660 and the flange 420, 620. As shown in FIG. 6B, the raised aperture housing 600 includes a raised aperture portion 662 that extends from the plane of the base 660 so as to advantageously provide a larger spacing between the detector 820 and a tissue site, further reducing the effects of light piping.

[0040] FIGS. 7A-B illustrate an assembled pulse oximetry neonate sensor 700. The sensor 700 includes an optical end

701, an elongated body 703 and a connector end 705. The optical end 701 incorporates a detector assembly 1000 (FIGS. 10A-C), described below, including a low noise optical housing 400 (FIGS. 6A-B), as described above. The body 703 includes signal traces (not visible) between the optical end 701 and the connector end 705. The connector end 705 has a plug portion configured to insert into a mating patient cable connector so as to mechanically and electrically connect the sensor 700 to a patient cable 140 (FIG. 1), for example. A patient cable connector is described in U.S. Pat. No. 6,152,754 entitled "Circuit Board Based Cable Connector," which is assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

[0041] FIG. 7C illustrates an assembled pulse oximetry adult sensor 750. The sensor 750 includes an end wrap 751, a body 753 including an optical section 754, a middle wrap 755, and a connector end 759. The optical section 754 incorporates a detector assembly 1000 similar in construction to that described in FIGS. 10A-C, below, including a low noise optical housing 400 (FIGS. 6A-B), as described above. The sensor 750 includes signal traces (not visible) between the optical section 754 and the connector end 759. The connector end 759 is similar to that described with respect to FIGS. 7A-B, above. A pulse oximetry adult sensor having end and middle wraps and an electromagnetic interference (EMI) shield is described in U.S. patent application Ser. No. 10/137,942, filed May 2, 2002, entitled "Flex Circuit Shielded Optical Sensor," assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

[0042] FIGS. 8-12 illustrate assembly of a neonate sensor 700 (FIGS. 7A-B) and an adult sensor 750 (FIG. 7C) including component attachment (FIGS. 8A-B), detector EMI shielding and optical shielding (FIGS. 9-11), and tape stock assembly (FIGS. 12A-B). FIG. 8A illustrates a neonate sensor circuit assembly 800 including multiple, duplicate flexible circuit assemblies 801 each having a flexible circuit substrate 810 and associated components soldered or otherwise electrically connected to the flexible circuit substrate 810, as is well known in the art. Each flexible circuit assembly 801 includes a detector 820 and an emitter 830. The detector 820 is enclosed in an EMI shield 1010, described in further detail with respect to FIGS. 10A-C, below. The emitter 830 is connected to a pad 1110 having multiple contact sets, described in further detail with respect to FIG. 11A, below. Each assembly 801 may also include an information element 840, which can be read by an attached pulse oximeter 160 (FIG. 1). The information element 840 may provide information regarding the sensor 700, such as sensor type or manufacturer to name a few. An information element is described in U.S. Pat. No. 6,397,091, entitled "Manual and Automatic Probe Calibration," assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

[0043] FIG. 8B illustrates an adult sensor circuit assembly 850 likewise including multiple, duplicate flexible circuit assemblies 851 each having a flexible circuit substrate 860 and associated components soldered or otherwise electrically connected to the flexible circuit substrate 860, including a detector 820, an emitter 830 and maybe an information element 840, such as described with respect to FIG. 8A, above. The detector 820 is enclosed in an EMI shield 1010, such as described with respect to FIGS. 10A-C, below. In

one embodiment, the emitter **830** is connected to a pad **1160** (FIGS. **11C-E**) having extended contacts, as described below.

[0044] FIGS. **9A-B** illustrate a neonate sensor assembly **900** having a flexible circuit assembly **801**, a low noise optical housing **400** and a connector tab **910**. The sensor assembly **900** is configured as an optical portion **1100**, which is described in further detail with respect to FIGS. **11A-B**, below, and a connector portion **901**. The optical portion **1100** has an emitter **830** and a shielded detector assembly **1000**, described in further detail with respect to FIGS. **10A-C**. The connector portion **901** is configured with the connector tab **910** supporting sensor pinouts **920**.

[0045] FIGS. **9C-D** illustrate an adult sensor assembly **950** having a flexible circuit assembly **851**, a low noise optical housing **400** and a connector tab **910**. The sensor assembly **950** is configured as an optical portion **1150**, described in further detail with respect to FIGS. **11C-E**, below, and a connector portion **901**, as described above. The optical portion **1150** has an emitter **830** and a shielded detector assembly **1000**, such as is described in detail with respect to FIGS. **10A-C**.

[0046] FIGS. **10A-C** illustrate a shielded detector assembly **1000** configured for the neonate flexible circuit assembly **801** (FIGS. **8A, 9A-B**) as shown, or, similarly, for the adult flexible circuit assembly **851** (FIGS. **8B, 9C-D**). As shown in FIG. **10A**, inside pressure sensitive adhesive (PSA) **1020** and top PSA **1030** are removed from a foldable shield **1010**, and bottom PSA **1040** is removed from a fixed shield **1005** (not visible). As shown in FIG. **10B**, the shield **1010** is next folded toward the detector **820**. As shown in FIG. **10C**, the shield **1010** is then folded over the back and sides of the detector **820**, enclosing the detector **820**. The inside PSA **1020** adheres to the detector **820**, maintaining the foldable shield **1010** in place. Next, the EMI shielded detector **820** is placed into the optical housing **400**. The top PSA **1030** adheres to the inside surface of the optical housing **400**, which defines a pocket **440** (FIGS. **4BC**) as described above. The bottom PSA **1040** adheres to the optical housing base **410** (FIGS. **4A-C**), maintaining the detector **820** in place within the optical housing cover **410** (FIGS. **4AC**), aligned with the aperture **470** (FIG. **4A**), and maintaining the optical housing **400** in the closed position **560** (FIGS. **5C-D**).

[0047] FIGS. **11A-B** illustrate one embodiment of the optical portion **1100** of a sensor assembly **900** (FIGS. **9A-B**) having a detector assembly **1000** and an emitter **830** connected to a pad **1110**. As shown in FIG. **11A**, a particular embodiment of the pad **1110** advantageously has an inner contact set **1112** and an outer contact set **1114**. The emitter **830** may be attached and electrically connected in a first position to the inner contact set **1112** or in a second position to the outer contact set **1114**. As shown in FIG. **11B**, this advantageously provides two different detector-emitter spacings **1131, 1132** on the same flexible circuit substrate. A comparatively wider spacing **1131** corresponds to the second emitter position attached to the outer contact set **1114** (shown), and a comparatively narrower spacing **1132** corresponds to the first emitter position attached to the inner contact set **1112** (not shown). The choice of mounting the emitter with a narrower or wider spacing accommodates different sensor types for different sized patients or different tissue site thicknesses with fewer unique sensor parts or

subassemblies. Note that the detector **820** (FIGS. **10A-B**) is not visible in FIG. **11B** as it is behind the fixed shield **1005**. As an example, a neonate sensor **700** (FIGS. **7A-B**) and an infant sensor (not illustrated) configured for different sized foot sites may be manufactured from a single flex circuit part. In a preferred embodiment, the inner pads are configured for a 20 mm detector-emitter spacing appropriate for a neonate, such as a child weighing under 3 kg and the outer pads **1114** are configured for a 25 mm detector-emitter spacing appropriate for an infant, such as a child weighing 3-10 kg.

[0048] In another embodiment of the optical portion **1100**, a reinforcing tape (not shown) is applied to the component side (shown in FIG. **11A**) of the flexible circuit between the detector assembly **1000** and the emitter **830** so as to increase the number of bend cycles before failure of that flexible circuit area and to improve electrostatic discharge (ESD) resistance. The reinforcing tape is disposed over at least the extent of the pad **1110**. In a particular embodiment, the reinforcing tape is 0.004 inch polypropylene.

[0049] FIGS. **11C-E** illustrate one embodiment of the optical portion **1150** of a sensor assembly **950** (FIGS. **9C-D**) having a detector assembly **1000** and an emitter **830** connected to a pad **1160** having extended contacts. The contacts are extended along the direction between the detector assembly **1000** and the emitter **830**, allowing the emitter to be mounted on the same pad **1160** in multiple positions. As shown in FIG. **11C**, the emitter **830** is installed over an elongated aperture **1170**. The extended pad area **1160** advantageously provides for different detector-emitter spacings **1181, 1182** (FIGS. **11D-E**) on the same flexible circuit substrate. A comparatively narrower spacing **1181** corresponds to a first emitter position (FIG. **11D**), and a comparatively wider spacing **1182** corresponds to a second emitter position (FIG. **11E**). This accommodates different sensor types for different sized patients or different tissue site thicknesses with fewer unique sensor parts or subassemblies. As an example, an adult sensor **750** (FIGS. **7C**) and a pediatric sensor (not shown) configured for different sized finger sites may be manufactured from a single flex circuit part. As shown in FIGS. **11D-E**, in a preferred embodiment, the pad **1160** (FIG. **11C**) is configured with contacts that are extended at least 0.1 inches beyond an emitter **830** nominal lead length so as to accommodate a 1.0 inch detector-emitter spacing **1181** appropriate for a pediatric sensor or a 1.1 inch detector-emitter spacing **1182** appropriate for an adult sensor. The elongated aperture **1170** (FIG. **11C**) is configured accordingly, i.e. is elongated from a circular aperture sufficiently to accommodate either a 1.0 inch or a 1.1 inch detector-emitter spacing.

[0050] The ability to adjust the detector-emitter spacing on a particular flexible circuit so as to minimize the number of unique parts in manufacturing various sensor types and sizes is disclosed above. That disclosure is with respect to a pad **1110** (FIG. **11A**) having multiple contact sets and a pad **1160** (FIG. **11C**) having extended contacts with an associated elongated aperture **1170** (FIG. **11C**). One of ordinary skill in the art will recognize other electrical and mechanical structures that allow such detector-emitter spacing adjustment. For example, although adjustment of the emitter **830** location relative to the detector **820** is achieved by the above-disclosed embodiments, adjustment of the detector **820** location relative to the emitter **830** may be achieved with

similar structures. Further, adjustment of the detector-emitter spacing may also be achieved by altering the orientation of the detector **820** and/or the emitter **830**. These adjustments may also be accommodated by multiple apertures rather than an elongated aperture. Although the sensors disclosed are based upon the detection of light transmitted through a tissue site, the ability to adjust detector-emitter spacing is equally applicable to reflectance sensors, i.e. sensors that are based upon the detection of light reflected from a tissue site.

[0051] FIG. 12A illustrates a tape stock assembly **1200** for a neonate sensor. In particular, multiple sensor assemblies **900** are sandwiched between a base stock **1210** and a face stock **1220**. Individual completed sensors **700** (FIGS. 7A-B) are then cut from the tape stock assembly **1200**. A base stock and a face stock are described in U.S. Pat. No. 5,782,757, cited above.

[0052] FIG. 12B illustrates a tape stock assembly **1250** for an adult sensor. In particular, multiple sensor assemblies **950** are sandwiched between a base stock **1210** and a face stock **1220**. Individual completed sensors **750** (FIGS. 7C) are then cut from the tape stock assembly **1250**.

[0053] The low noise optical housing has been disclosed in detail in connection with various embodiments. These embodiments are disclosed by way of examples only and are not to limit the scope of the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications.

[0054] Additionally, all publications, patents, and patent applications mentioned in this specification are herein incorporated by reference to the same extent as if each individual publication, patent, or patent application was specifically and individually indicated to be incorporated by reference.

What is claimed is:

1. An optical housing comprising:

a substrate having a reflective side and an absorptive side;
a generally planar base portion of said substrate; and

a protruding cover portion of said substrate, said cover portion defining a pocket on said absorptive side;

said substrate having an open position with said base portion distal said cover portion and a closed position with said base portion proximate said cover portion, said substrate configured to enclose a detector within said pocket in said closed position;

wherein said base portion defines an aperture generally centered within said base portion and aligned with said detector in said closed position so as to pass light through to said detector.

2. The optical housing according to claim 1 further comprising a generally planar flange portion of said substrate disposed around the periphery of said cover portion.

3. The optical housing according to claim 2 wherein said base portion further defines a slot partially extending across said base portion proximate said flange portion, said substrate being foldable along said slot so as to move said substrate from said open position to said closed position.

4. The optical housing according to claim 3 wherein said substrate further comprises:

a first width across said base portion;

a second width across said flange portion, wherein said first width is narrower than said second width so as to seal the edges of said substrate in said folded position; and

a plurality of indents generally aligned with said slot defining a transition from said first width to said second width.

5. The optical housing according to claim 4 wherein said substrate has a length that is less than about 1.1 inches and said second width is less than about 0.4 inches.

6. The optical housing according to claim 1 wherein said substrate comprises a laminate having a generally white layer corresponding to said reflective side and a generally black layer corresponding to said absorptive side.

7. The optical housing according to claim 1 further comprising a raised aperture portion of said substrate that extends from the plane of said base portion so as to provide spacing between said detector and a tissue site.

8. An optical housing method comprising the steps of:

providing a substrate having an absorptive side and a reflective side;

forming a cover portion of said substrate so as to create a pocket on said absorptive side;

punching said substrate so as to separate a housing from said substrate;

securing a detector within said pocket; and

enclosing said detector with said housing.

9. The optical housing method according to claim 8 wherein said providing step comprises the substep of laminating a white layer and a black layer.

10. The optical housing method according to claim 8 wherein said forming step comprises the substeps of:

creating a ramp sloping from a flange disposed around the periphery of said cover to a raised platform; and

beveling sides that slope from said flange to said platform.

11. The optical housing method according to claim 8 wherein said punching step comprises the substep of shaping a base adapted to fold over said pocket.

12. The optical housing method according to claim 11 wherein said punching step comprises the further substep of shaping a flange around the periphery of said base, said flange having indents that taper from a wider flange width to a narrower base width.

13. The optical housing method according to claim 12 wherein said punching step comprises the further substep of defining an aperture generally centered within said base.

14. The optical housing method according to claim 13 wherein said punching step comprises the further substep of defining a slot partially extending across said base width proximate said flange.

15. The optical housing method according to claim 8 wherein said securing step comprises the substep of adhering a detector assembly incorporating said detector to an inside surface of said housing that defines said pocket.

16. The optical housing method according to claim 11 wherein said enclosing step comprises the substep of folding

said base from an open position distal said flange to a closed position proximate said flange.

17. An optical housing comprising:

a light reflecting cover means for shielding against ambient light;

a base means for blocking piped light, said base means adjoining said cover means;

a light absorbing pocket means for securing a detector, said pocket means defined by said cover means and said base means; and

an aperture means for allowing light transmitted through a tissue site to be received by said detector, said aperture means defined by said base means.

18. The optical housing according to claim 17 further comprising a slot means for moving said base means between an open position configured for placing said detector in said pocket means and a closed position configured for enclosing said detector within said pocket means.

19. The optical housing according to claim 17 further comprising a laminate means for forming said cover means and said base means from a single substrate, said laminate means having a reflective side corresponding to said cover means and an absorptive side corresponding to said pocket means.

20. The optical housing according to claim 17 further comprising a flange means disposed around said cover means adapted to attach said housing to a tape stock layer of a disposable sensor.

21. A sensor circuit comprising:

a circuit substrate;

a pair of pads disposed on an optical portion of said circuit substrate;

a plurality of pinouts disposed on a connector portion of said circuit substrate; and

a plurality of conductive paths providing electrical communication between said pads and said pinouts, said pads configured to mechanically mount a corresponding pair of optical components to said circuit substrate and to electrically connect said components to said conductive paths, at least one of said pads adapted to mount one of said components at either a first spacing or a second spacing from the other one of said components, said second spacing being greater than said first spacing by a predetermined amount.

22. The sensor circuit according to claim 21 wherein said at least one of said pads comprises a plurality of extended contacts providing a first attachment position corresponding to said first spacing and a second attachment position corresponding to said second spacing.

23. The sensor circuit according to claim 21 wherein said at least one of said pads comprises a first contact set of contacts corresponding to said first spacing and a second contact set corresponding to said second spacing, said first contact set and said second contact set being electrically connected in parallel.

24. The sensor circuit according to claim 21 further comprising an elongated aperture defined by said substrate and adapted to transmit light through said substrate for said one of said components mounted at either said first spacing or said second spacing.

25. The sensor circuit according to claim 21 wherein said first spacing is about 20 mm and said second spacing is about 25 mm.

26. The sensor circuit according to claim 21 wherein said first spacing is about 1.0 inch and said second spacing is about 1.1 inch.

27. A sensor circuit comprising:

a flexible circuit substrate;

a first pad disposed on said substrate and configured to mount a detector; and

a second pad disposed on said substrate and configured to mount an emitter, at least one of said first pad and said second pad adapted so that a detector-emitter spacing is a first distance or a second distance depending on the placement of at least one of said detector and said emitter,

said first distance and said second distance predetermined so as to accommodate particular sensor types.

28. The sensor circuit according to claim 27 wherein:

said second pad comprises a first contact set and a second contact set,

said emitter mountable to said first contact set said first distance from said detector mounted to said first pad, and

said emitter mountable to said second contact set said second distance from said detector mounted to said first pad.

29. The sensor circuit according to claim 27 wherein:

said second pad comprises a plurality of extended contacts,

said emitter mountable to said contacts in a first position located a first distance from said detector mounted to said first pad, and

said emitter mountable to said contacts in a second position located a second distance from said detector mounted to said first pad.

30. The sensor circuit according to claim 29 further comprising an elongated aperture configured so that light is transmitted from said emitter through said aperture when said emitter is mounted in either said first position or said second position.

31. The sensor circuit according to claim 27 wherein said sensor types comprise a neonate sensor and an infant sensor, said first distance and said second distance in the range of about 20 mm to about 25 mm.

32. The sensor circuit according to claim 27 wherein said sensor types comprise a pediatric sensor and an adult sensor, said first distance and said second distance in the range of about 1.0 in. to about 1.1 in.

33. A sensor circuit method comprising the steps of:

predetermining a plurality of optical component spacings based upon a corresponding plurality of sensor types, said sensor types indicative of tissue site location and patient size;

configuring a pad to fixedly mount and electrically connect an optical component to a flexible circuit at a plurality of positions, said positions corresponding to said spacings; and

mounting said optical component to a particular one of said positions to construct a particular one of said sensor types.

34. The sensor circuit method according to claim 33 comprising the further step of adapting at least one aperture defined by said flexible circuit so as to pass light for said optical component mounted at any of said positions.

35. The sensor circuit method according to claim 33 wherein said configuring step comprises the substep of constructing a plurality of contact sets electrically connected in parallel, each of said sets providing a corresponding one of said positions.

36. The sensor circuit method according to claim 33 wherein said configuring step comprises the substep of providing a plurality of contacts extending from said optical component so that said optical component is mountable to said contacts in each of said positions.

37. A sensor comprising:

a circuit substrate means for mounting and electrically connecting components;

a pad means disposed on said substrate for fixedly mounting an emitter at either a first spacing or at a second spacing from a detector; and

a tape stock means for attaching said emitter and said detector to a tissue site.

38. The sensor according to claim 37 further comprising an aperture means for passing light from said emitter through said circuit substrate with said emitter mounted at either said first spacing or said second spacing.

39. The sensor according to claim 38 further comprising a tape means disposed over said pad means so as to improve bend cycles and ESD resistance.

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